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㉙ Oxygen carrier.

㉚ A modified haemoglobin for use as an oxygen carrier in a blood substitute is prepared by covalently bonding haemoglobin or a haemoglobin derivative to a polyalkylene glycol, via an amide bond. A carboxyl group is first introduced onto the polyalkylene glycol, and is then reacted with an amino group of the haemoglobin or haemoglobin derivative to form the amide bond.

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OXYGEN CARRIER

The present invention relates to a modified haemoglobin for use as an oxygen carrier in a blood substitute.

It is known that haemoglobin covalently bonded to
5 a polymer selected from polyethylene glycol,
polypropylene glycol and copolymers of ethylene
oxide and propylene oxide, is useful as an oxygen
carrier for a blood substitute (see JP-12308/1981-A
and US-4301144-A).

10 According to the present invention, there is provided
an oxygen carrier comprising haemoglobin or a haemoglobin
derivative covalently bonded to a polymer (such as a
polyalkylene glycol or polyether), characterised in that
the haemoglobin or haemoglobin derivative is covalently
15 bonded to said polymer via an amide bond.

The present invention also provides a method of
preparing an oxygen carrier, which comprises introducing
at least one carboxyl group onto a polymer and
covalently bonding the polymer to haemoglobin or a
20 haemoglobin derivative by reaction of an amino group
of the haemoglobin or haemoglobin derivative with the
carboxyl group of the polymer to form an amide bond.

The improvement in accordance with the invention is
that the haemoglobin or haemoglobin derivative is
25 attached to the polymer by an amide bond.

The polymer used in the present invention is, for
example, (a) a polyalkylene glycol (i.e. a polyether)

selected from polyethylene glycol, polypropylene glycol and copolymers of ethylene oxide and propylene oxide; (b) an ether of one of the foregoing polyalkylene glycols and an alcohol having from 1 to 16 carbon atoms (examples of such ethers being the monomethyl, monocetyl and monooleyl ethers); (c) an ester of one of the foregoing polyalkylene glycols and a carboxylic acid having from 2 to 18 carbon atoms (examples of such esters being the monobutyl and monostearyl esters); and 10 (d) a dehydrated product of one of the foregoing polyalkylene glycols and an amine having from 1 to 18 carbon atoms (example of such amines being propyl amine and stearyl amine). The molecular weight of the polymer, e.g. polyether, is preferably from 300 to 20000, more 15 preferably from 750 to 10000, from the point of view of efficiency and viscosity.

As a process for introducing carboxylic groups into the polymer, there can be employed, for example, (a) the known method described in US-4179337-A and US-3941710-A, 20 and (b) the method which comprises attaching at least one carboxylic acid or polycarboxylic acid (such as an alkane dicarboxylic acid) to a terminal hydroxyl group of the polyether to give an ester.

In order to react the polymer into which the 25 carboxyl group has been introduced with haemoglobin or a derivative thereof, there can be employed, for example, (a) a method which comprises converting the polymer into a conventional peptide synthesis product (such as by reaction with N-hydroxysuccinimide, N-hydroxyphthalimide, 30 p-nitrophenol or pentachlorophenol) and reacting the product with haemoglobin or a derivative thereof so as to form an amide bond, or (b) a method which comprises treating the carboxylated polyether with a halogenating agent such as thionyl chloride to give an acid halide 35 of the polymer having at least one carboxyl group and then combining this product with haemoglobin or a derivative thereof.

Examples of the polycarboxylic acids mentioned above are malonic acid, succinic acid, glutaric acid, adipic acid, malic acid and citric acid. The oxygen carrying ability of the haemoglobin-polymer complexes of the present invention are not reduced by the presence of carboxylic groups in the complex.

The haemoglobin used in the present invention includes haemoglobin obtained from animals such as cattle, swine, sheep, horses, dogs, monkeys and chickens, as well as from human beings, and further includes haemoglobin derivatives such as the pyridoxal-5'-phosphate derivative, the pyridoxal-5'-sulphate derivative, the 2-nor-2-formyl pyridoxal-5'-phosphate derivative, the 2,3-diphosphoglyceric acid derivative, the inositol hexaphosphate derivative, the inositol pentaphosphate derivative, or a derivative derived from a sugar containing a carboxylic or phosphate group.

In the haemoglobin-polymer complexes of the present invention, the number of the polymer attached (substitution degree) and molecular weight of a given complex can be determined by the method of Ajisaka et al (K. Ajisaka and Y. Iwashita, Biochem. Biophys. Res. Commun. 97, 1076-1081, 1981): Thus, for example, from 1 to 20 molecules of polyether carboxylic acid are attached to a given haemoglobin (subunit).

The haemoglobin-polymer complex is preferably prepared according to one of the following methods (1), (2) and (3).

(1) The polyether carboxylic acid and from 1 to 10 mol, preferably 2 mol, of N-hydroxysuccinimide are dissolved in N,N-dimethylformamide in the presence of from 1 to 10 mol, preferably 2 mol, of dicyclohexyl-carbodiimide, and reacted for 3 to 20 hours, preferably 8 to 14 hours, at room temperature or with heating.

35 The dicyclohexylurea which precipitates is removed by filtration. By adding ethyl ether to the filtrate an activated ester is obtained. The ester is allowed to react with about 1 to

1/100 mol, preferably 1/5 to 1/30 mol, of haemoglobin or haemoglobin derivative at a pH of 6.5 to 9.5, preferably 7 to 8.5, in an aqueous solution or in a buffer solution. In the first reaction, N-hydroxyphthalimide, p-nitrophenol or pentachlorophenol may be used in place of N-hydroxysuccinimide, whereby almost the same results are obtained.

(2) The polyether carboxylic acid and from 1 to 10 mol, preferably 5 mol, of imidazole are dissolved in 10 N,N-dimethylformamide. To this mixture, from 1 to 10 mol, preferably 5 mol, of dicyclohexylcarbodiimide are added, and the mixture is reacted for 5 to 20 hours, preferably 10 hours, under reflux. After the mixture has cooled, the resulting dicyclohexyl urea is removed 15 by filtration. By adding ethyl ether to the filtrate, an activated polyether carboxylic acid ester is obtained. This activated polyether carboxylic acid ester is allowed to react with about 1 to 1/100 mol, preferably 1/5 to 1/30 mol, of haemoglobin or haemoglobin derivative at 20 a pH of 7 to 9, preferably 7.5 to 8.5, in an aqueous solution or in a buffer solution. In the second reaction, succinimide or phthalimide may be used in place of imidazole, whereby almost the same results are obtained. In order to activate the polyether carboxylic acid, it 25 may be allowed to react with 1 to 10 mol, preferably 2 mol, of carbonyldiimidazole in N,N-dimethylformamide.

(3) The polyether carboxylic acid is reacted with an excess of thionyl chloride for 1 to 5 hours, preferably 1.5 to 2 hours, at a temperature of 60 to 30 90°C, preferably 75 to 80°C. Thionyl chloride is removed by distillation under reduced pressure, and the resulting polyether carboxylic acid halide is allowed to react with 1/10 to 1/100 mol, preferably 1/30 to 1/50 mol, of haemoglobin or haemoglobin derivative at a 35 pH of 8.5 to 9.5, in an aqueous solution or in a buffer solution. In the first reaction, another acid halogenating agent such as phosphorus oxychloride or

phosphorus pentachloride may be used in place of thionyl chloride.

The safety of the modified haemoglobin of the present invention has been proved by exchange transfusion experiments. Thus, when more than 90% of the blood of rats was exchange transfused with a 6% solution of a modified haemoglobin of the present invention, the rats survived, whereas, when the blood of rats was exchange transfused with 6% bovine serum albumin solution, the rats died before the exchange ratio reached 82%. This result proves the absence of any acute toxicity of the modified haemoglobin of the present invention, whose LD₅₀ is estimated to be over 4.5g/kg.

The present invention is illustrated by the following Examples and Experiments.

Example 1

5g (0.001 mol) of monomethoxy polyethylene glycol succinate having a mean molecular weight of 5000 and 0.23g (0.002 mol) of dicyclohexylcarbodiimide were dissolved in 300ml of N,N-dimethylformamide. The mixture was stirred overnight at room temperature.

The dicyclohexylurea which precipitated was separated by filtration. To the filtrate, 600ml of ethyl ether were added, whereby monomethoxy polyethylene glycol mono(succinimidyl succinate) separated in a crystalline form. The crystals were separated by filtration and washed with ethyl ether, whereby 4.6g of white crystalline material were obtained.

0.5g (0.1 millimol) of the activated polyether ester was added at 0°C to a solution obtained by dissolving 0.5g (0.0077 millimol) of the haemoglobin derivative of pyridoxal-5'-phosphate in 100ml of phosphate buffer solution of pH 8.5. The mixture was stirred for 4 hours at 0°C. The product was purified by repeated ultrafiltration using a membrane whose molecular weight cut-off point was 30000 daltons, whereby unreacted activated ester and decomposed materials

were removed, and a solution of a modified haemoglobin was obtained. The modified haemoglobin solution had a single peak when subjected to high speed liquid chromatography using a TSK G3000 SW column (Toyo Soda Co., Inc. Japan).

The solution was freeze-dried, whereby 0.58g of modified haemoglobin was obtained. This modified haemoglobin had a substitution degree of 6.0 and a molecular weight of 95000. The substitution degree and molecular weight were estimated assuming that the modified haemoglobin had formed a tetramer ($\alpha_2\beta_2$).

Example 2

2g (1 millimol) of polyethylene glycol adipate having a mean molecular weight of 2000, 0.27g (1 millimol) of pentachlorophenol and 0.25g (1.2 millimol) of dicyclohexylcarbodiimide were added to 30ml of N,N-dimethylformamide, and the mixture was left overnight at room temperature. The dicyclohexylurea which precipitated was filtrated off. The crystalline material which was precipitated by adding ethyl ether to the filtrate was separated by filtration, and was re-crystallized from toluene to give 1.5g of crystalline material.

0.22g (0.1 millimol) of the activated ester thus prepared was added slowly to 20ml of 0.05% aqueous carbonylhaemoglobin solution. The pH of the solution was kept at 8.5 with 0.2N aqueous sodium hydroxide solution.

The reaction mixture was subjected to repeated ultrafiltration using a membrane whose molecular weight cut-off point was 30000 daltons, whereby 2ml of a 0.4% modified haemoglobin solution was obtained. The modified haemoglobin had a single peak when subjected to high speed liquid chromatography, and had a substitution degree of 3.5 and a molecular weight of 72000.

Example 3

8.5g (0.015 mol) of polyethylene glycol monocarboxy-

methyl ether having a mean molecular weight of 850,
2.07g (0.015 mol) of p-nitrophenol and 2.3g (0.015 mol)
of dicyclohexylcarbodiimide were dissolved in 300ml of
N,N-dimethylformamide, and reacted overnight at room
5 temperature.

Dicyclohexylurea was separated by filtration, and
600ml of ethyl ether were poured into the filtrate to
form 6.2g of crystalline material.

The activated ester thus prepared was reacted with
10 10ml of the haemoglobin derivative of glucose-6-
phosphate (1% solution) in the same manner as in
Example 1, whereby 10.5 ml of a 0.8% modified
haemoglobin solution were obtained. The modified
haemoglobin has a substitution degree of 6.2 and a
15 molecular weight of 70000.

Example 4

4g (0.002 mol) of monomethoxy polyethylene glycol
succinate (molecular weight 2000) and 0.7g (0.004 mol)
of N,N-carbodiimidazole were dissolved in 100ml of
20 N,N-dimethylformamide and allowed to react overnight
at room temperature. 200ml of ethyl ether were poured
into the reaction mixture and the precipitate was
separated by filtration and washed well with ethyl
ether to give monomethoxy polyethylene glycol imidazolyl
25 succinate (yield: 2.2g).

6ml (0.0055 millimol) of 6% solution of the
haemoglobin derivative of pyridoxal-5'-phosphate were
added to 60ml of 0.1M Tris buffer solution of pH 8.0,
and to the solution, 1g (0.5 millimol) of the above
30 imide was added.

After 4 hours reaction in an ice bath, the product
was subjected to repeated ultrafiltration using a
membrane whose molecular weight cut-off point was
30000 daltons, whereby 3.6ml of an 8.3% aqueous modified
35 haemoglobin solution were obtained. The modified
haemoglobin had a substitution degree of 10.4 and a
molecular weight of 86000.

Example 5

5g (0.001 mol) of monomethoxy polyethylene glycol succinate (molecular weight 5000); 0.5g (0.005g mol) of succinimide and 1g (0.005 mol) of dicyclohexylcarbodi-
5 imide were dissolved in 50ml of N,N-dimethylformamide, and the reaction mixture was refluxed for 12 hours.

The dicyclohexylurea which precipitated was filtrated off. To the filtrate, 150ml of ethyl ether was added, and the resulting precipitate was separated by
10 filtration. The precipitate was washed well with ethyl ether and dried to give 3.2g of crystalline material.

3.8ml of a 4.8% modified haemoglobin solution was obtained by the reaction of the above imide with 7ml of the haemoglobin derivative of pyridoxal-5'-phosphate
15 (concentration 3.2%) by the same procedure as in Example 4. The modified haemoglobin had a substitution degree of 11.2 and a molecular weight of 120000.

Example 6

5g (0.001 mol) polyethylene glycol monocarboxymethyl
20 ether having a mean molecular weight of 5200 was dissolved in 20ml of thionyl chloride and heated for 1.5 hours at a temperature of 75~80°C.

Unreacted thionyl chloride was removed by distillation under reduced pressure. The resulting
25 acid chloride salt in crystalline form was dried well. 20 ml of a 1% solution of the carbonylhaemoglobin derivative of pyridoxal-5'-phosphate was dissolved in 200 ml of 0.7M borate buffer solution of pH 10.0. To the solution, 5g of the above acid chloride were added
30 slowly at 0°C.

After 3 hours' stirring at 0°C, the reaction mixture was subjected to repeated ultrafiltration using a membrane whose molecular weight cut-off point was 50000 daltons, whereby 4.6ml of a 4.1% modified
35 haemoglobin solution was obtained. The modified haemoglobin had a substitution degree of 9.3 and a molecular weight of 114000.

Example 7

100g (0.025 mol) of polyethylene glycol (molecular weight 4000) and 6.3g (0.063 mol) of succinic acid anhydride were dissolved in 100ml of N,N-dimethylformamide.

5 The mixture was stirred for 3 hours at 100°C, and the reaction mixture was then cooled.

To the mixture, 400ml of ethyl ether were added, and the resulting precipitate was separated by filtration, washed well with ethyl ether, and dried to give 97.5g of
10 polyethylene glycol disuccinate in the form of a crystalline material.

97.5g (0.024 mol) of the crystalline material, 6.3g (0.054 mol) of N-hydroxysuccinimide, and 11.4g (0.054 mol) of dicyclohexylcarbodiimide were dissolved
15 in 100ml of N,N-dimethylformamide with heating, and the mixture was then stirred overnight at 30°C. The dicyclohexylurea which precipitated was separated by filtration.

Polyethylene glycol bis(succinimidyl succinate) in a
20 crystalline form, produced by adding 300 ml of ethyl ether to the filtrate, was separated by filtration, washed well with ethyl ether and dried to give 95g of a white crystalline material.

10ml (0.025 millimol) of a 16.4% haemoglobin solution
25 was poured into 35ml of borate buffer solution of pH 8.5. To the mixture, 4.3g (1.0 millimol) of the crystalline polyethylene glycol bis(succinimidyl succinate) were added. The mixture was stirred overnight at 4°C.

The product was purified by repeated ultrafiltration
30 using a membrane whose molecular weight cut-off point was 100000 dalton, whereby 51ml of a 3.2% modified haemoglobin aqueous solution were obtained. The modified haemoglobin had a substitution degree of 11.2 and a molecular weight of 122000.

35 Exrmple 8

14.3ml (0.1 millimol) of a 15% solution of the haemoglobin derivative of pyridoxal-5'-phosphate was

added to 270ml of phosphate buffer solution of pH 7.0. To this solution, 4.43g (1.1 millimol) of crystalline polyethylene glycol bis (succinimidyl succinate) were added slowly at 4°C.

5 The mixture was stirred for 4 hours at 4°C, and then the product was purified by repeated ultrafiltration using a membrane whose molecular weight cut-off point was 100000 daltons, whereby 11ml of a 11.6% modified haemoglobin solution were obtained. The modified
10 haemoglobin had a substitution degree of 6.6 and a molecular weight of 93000.

Experiment 1

15 The oxygen dissociation curves of the haemoglobin-polyether complexes prepared in accordance with the above Examples were determined by the method of Imai et al (K. Imai, H. Morimoto, M. Kotani, H. Watari, H. Waka and M. Kuroda; Biochim. Biophys. Acta, 200, 189-196, 1970), and therefrom the oxygen partial pressure at which half of the haemoglobin is saturated with
20 oxygen (P_{50} value), was estimated. The results are given in Table 1.

25 By use of the same haemoglobin-polyether complexes, the residence time in the circulatory system of rats was measured as follows. Two rats (weight about 350g) were used for each measurement. The rats were infused with 5ml of a 4-6% solution of the haemoglobin-polyether complex per kg of body weight through the femoral vein, and samples of blood, each 0.2ml, were withdrawn 5, 10, 15, 30, 60, 90 and 120 minutes after
30 the injection. Each blood sample was centrifuged, and the concentration of haemoglobin in the plasma was determined by the cyanomethemoglobin method.

35 The half residence time for each sample was estimated from a graph of the change in concentration against the time after the injection. The results are given in Table 1.

TABLE 1

	Example No.	P ₅₀ value ** (mm Hg)	Half Residence Time (minutes)
5	1	8.8	150
	2*	3.6	120
	3	4.3	150
	4	4.4	180
	5	9.8	250
	6*	3.1	220
10	7	3.0	170
	8	7.7	160
15	The haemoglobin polyether complex of Example 2 of US-4301144-A	13.5	120
	Haemoglobin, free (control)	8.7	35

*: Carbon monoxide was removed under an oxygen stream,
 20 and thereafter the P₅₀ value and half residence time
 were determined.

**: 25°C, pH 7.4, 0.1N NaCl
 From these results, it can be seen that the half
 residence times of the haemoglobin-polyether complexes
 25 of the Examples of the present invention in the
 circulatory systems of rats were from 4 to 7 times as
 long as that of haemoglobin itself. Furthermore, the
 complexes of the Examples of the present invention have
 a remarkable ability to deliver oxygen to the tissues
 30 of the organs.

Experiment 2

The Bohr Effect of the haemoglobin-polyether complex prepared in accordance with Example 2 of the present invention and in accordance with Example 4 of US-4301144-A, 35 were measured, according to the method of Bucci and Fronticelli (E.Bucci and C. Fronticelli, Method in Enzymology, Vol. 76, 523-533 (1981)). The results are

given in Table 2.

Table 2

Sample	Bohr coefficient*
Example 5 of this invention	0.33
Example 4 of US-4301144-A	0.12
Haemoglobin, free (Control)	0.48

* 25C, 0.1M phosphate buffer

From the results of Table 2, it can be seen that the Bohr Effect of the modified haemoglobin of Example 5 of the present invention was about 3 times larger than that of the modified haemoglobin of Example 4 of US-4301144-A. Consequently, the former has a superior ability in transporting carbon dioxide from the tissues to the lungs.

15 Experiment 3

The colloidal osmotic pressures of 6% solutions of the haemoglobin-polyether complexes prepared according to Examples 1, 7 and 8 of this invention and according to Example 6 of US-4301144-A, were measured. The results are given in Table 3.

Table 3

Sample	Colloidal Osmotic Pressure* (mm Hg)
Example 1 of this invention	39.4
Example 7 of this invention	42.5
Example 8 of this invention	38.8
Example 6 of US-4301144-A	156.6
Blood (control)	31.0

25 * The colloidal osmotic pressure was measured by a 4100 Colloid Osmometer (Wescor Inc.) at 25C.

30 From the above results, it can be seen that the colloidal osmotic pressure of the complexes of Examples 1, 7 and 8 of this invention renders the complexes more suitable for blood transfusion purposes than the complex of Example 4 of US-4301144-A. Thus, the complexes of Examples 1, 7 and 9 of the present invention are superior in their ability to carry carbon dioxide from the

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tissues to the lungs, and in their safety (because of their lower colloidal osmotic pressure). Therefore, the complexes are very useful for oxygen carriers in blood substitutes.

CLAIMS

1. An oxygen carrier comprising haemoglobin or a haemoglobin derivative covalently bonded to a polymer (such as a polyalkylene glycol or polyether), characterised in that the haemoglobin or haemoglobin derivative is covalently bonded to said polymer via an amide bond.
2. An oxygen carrier as claimed in claim 1, wherein said polymer is polyethylene glycol, polypropylene glycol or a copolymer of ethylene oxide and propylene oxide.
3. An oxygen carrier as claimed in claim 2, wherein one or at least one hydroxyl group of said polymer is substituted by (a) a radical derived from an alcohol having from 1 to 16 carbon atoms, (b) a radical derived from a carboxylic acid having from 2 to 18 carbon atoms, or (c) a radical derived from an amine having from 1 to 18 carbon atoms; or wherein said polymer is not substituted.
4. An oxygen carrier as claimed in any of claims 1 to 3, said amide bond having been formed by the use of a monohalogenated carboxylic acid, a dicarboxylic acid, or other carboxylic acid.
5. An oxygen carrier as claimed in any of claims 1 to 4, wherein the haemoglobin derivative is haemoglobin modified with pyridoxal or a derivative thereof, or with a sugar phosphate, or with 2,3-phosphoglyceric acid or a derivative thereof.
6. An oxygen carrier as claimed in claim 5, wherein the derivative is the pyridoxal-5'-phosphate derivative of haemoglobin, the pyridoxal-5'-sulphate derivative of haemoglobin, the 2-nor-2-formylpyridoxal-5'-phosphate derivative of haemoglobin, or the glucose-6-phosphate derivative of haemoglobin.

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7. An oxygen carrier as claimed in any claims 1 to 6, wherein said polymer has a molecular weight of from 300 to 20000.

8. An oxygen carrier as claimed in claim 7, wherein said polymer has a molecular weight of from 750 to 10000.

9. A method of preparing an oxygen carrier, which comprises introducing at least one carboxyl group onto a polymer and covalently bonding the polymer to haemoglobin or a haemoglobin derivative by reaction of an amino group of the haemoglobin or haemoglobin derivative with the carboxyl group of the polymer to form an amide bond.

10. A method according to claim 9, wherein the carboxyl group is introduced onto the polymer by reaction of the polymer with a dicarboxylic acid or a monohalogenated carboxylic acid.

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